

Factor number selection in the tensor decomposition of EEG data:

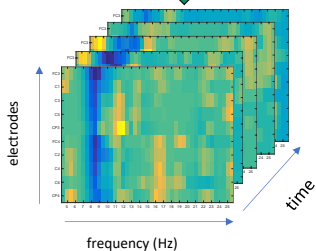
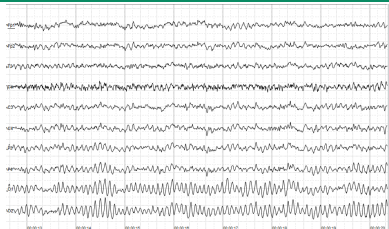
Mission (im)possible?

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MEASUREMENT 2021

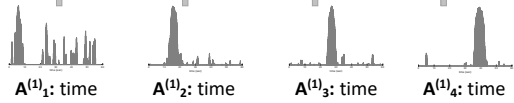
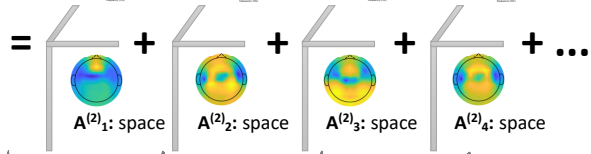
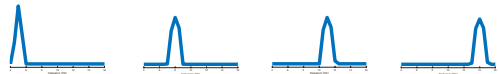
Parallel factor analysis (PARAFAC) and EEG



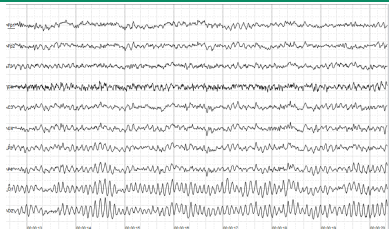
[Harshman, 1970]

Factor 1 Factor 2 Factor 3 Factor 4

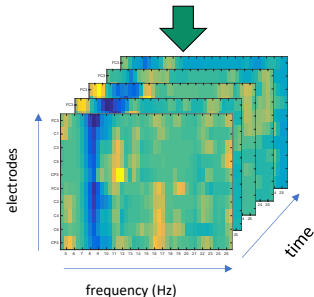
$A^{(3)}_1$: freq. $A^{(3)}_2$: freq. $A^{(3)}_3$: freq. $A^{(3)}_4$: freq.



Parallel factor analysis (PARAFAC) and EEG



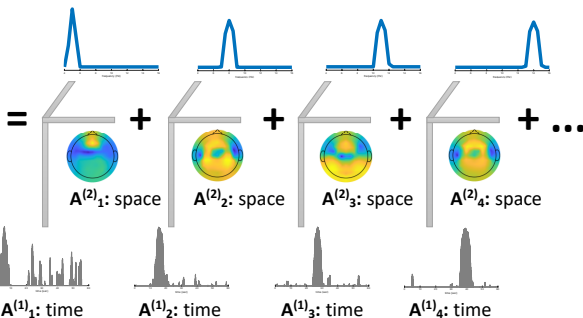
number of factors $F = ?$



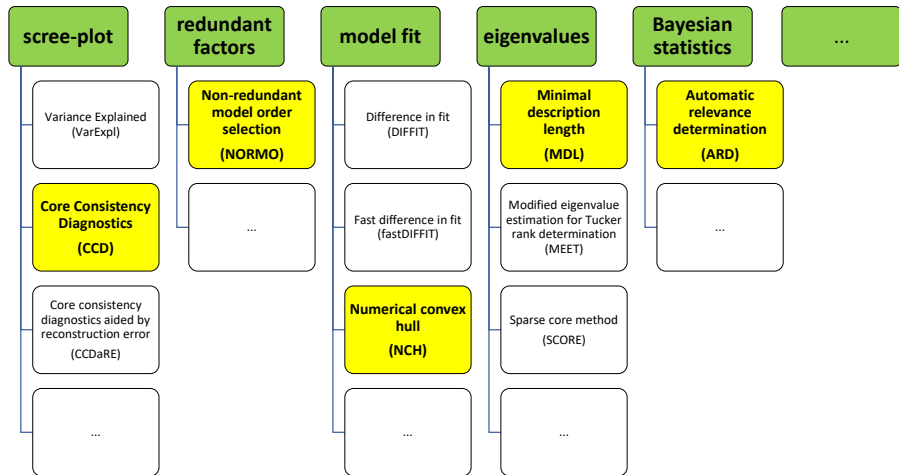
[Harshman, 1970]

Factor 1 Factor 2 Factor 3 Factor 4

$A^{(3)}_1$: freq. $A^{(3)}_2$: freq. $A^{(3)}_3$: freq. $A^{(3)}_4$: freq.



Factor number selection methods

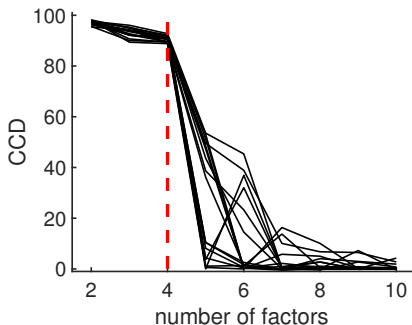


Core consistency diagnostics (CCD)

- [Bro and Kiers, 2003]
- Parallel factor analysis (PARAFAC) models with $f = 1, \dots, F_{max}$ factors

$$CCD(f) \in (-\infty, 100]$$

- an "elbow"/rapid change in the CCD decreasing profile

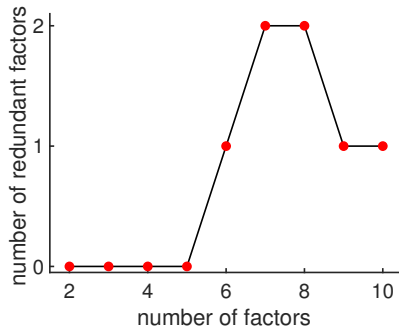


Non-redundant model order selection (NORMO)

- [Fernandes et al., 2020]
- PARAFAC models with $f = 1, \dots, F_{max}$ factors

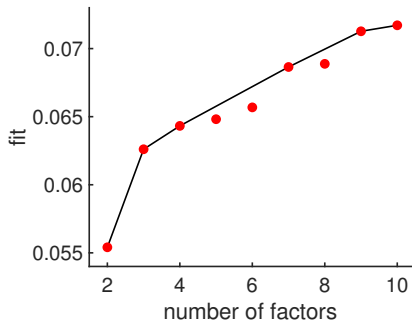
$NORMO(f)$ = number of redundant factors \rightarrow correlation > 0.7

- $F \rightarrow$ the **largest** f with $NORMO(f) = 0$ and $NORMO(f + 1) > 0$
- $NORMO_E/NORMO_B$ - all/selected PARAFAC models are considered



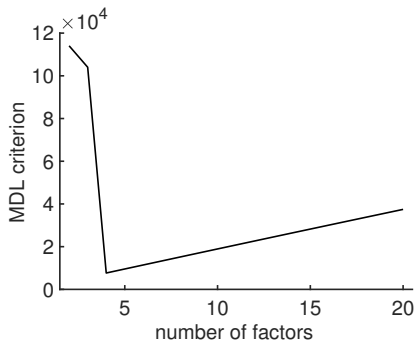
Numerical convex hull (NCH)

- [Ceulemans and Kiers, 2006]
 - PARAFAC models with $f = 1, \dots, F_{max}$ factors
 - maximal change in fit between models with a consecutive number of factors
- only models, which fit belongs to the fit convex hull boundary, are considered



Minimal description length (MDL)

- [Liu et al., 2016]
 - eigenvalues of matricized versions of the tensor
- ⇒ "indirect" assumption of factors orthogonality
- $F \in \operatorname{argmin}_{f \in \{2, \dots, F_{max}\}} \text{MDL}(f)$



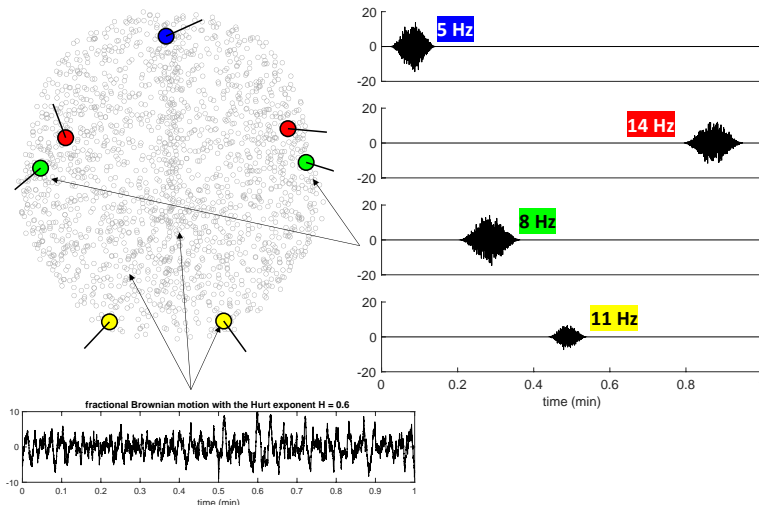
Automatic relevance determination (ARD)

- [Mørup and Hansen, 2009]
- factor elements are assumed to follow
 - **normal** distribution → **ridge** version of ARD (ARD_R)
 - **Laplacian** distribution → **sparse** version of ARD (ARD_S)
- **iterative algorithm:**
 - k^{th} step: PARAFAC model with F_k factors is estimated
 - factors with lowest weights are pruned out
 - ⇒ number of factors decreases to $F_{k+1} \leq F_k$
- modified selection criterion

Simulated EEG data

$$S_{EEG} = C \times S_{\text{source signal}}$$

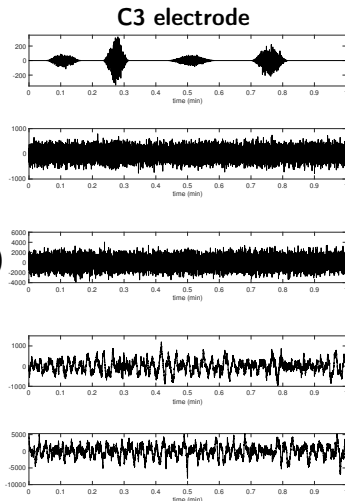
$64 \times T$ EEG signal 64×2004 forward model $2004 \times T$ (number of time points) oscillations + broadband brain activity



Simulated EEG data

- N_0 - only 4 oscillations
5 Hz, 8 Hz, 11 Hz, 14 Hz
- NG_{low} - N_0 + gaussian noise $\mathcal{N}(0, 200)$
- NG_{high} - N_0 + gaussian noise $\mathcal{N}(0, 1000)$
- $NBBA_{low}$ - 4 oscillations and "low" BBA
- $NBBA_{high}$ - 4 oscillations + "high" BBA

→ 20 sets for each type of data



Results

Mission 1 - N_0 data

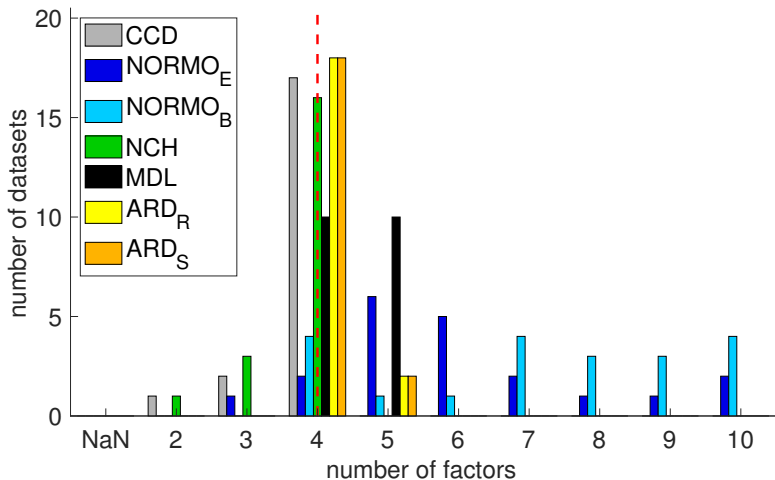
CCD

NORMO_E, NORMO_B

NCH

MDL

ARD_R, ARD_S



Mission 1 - N_0 data

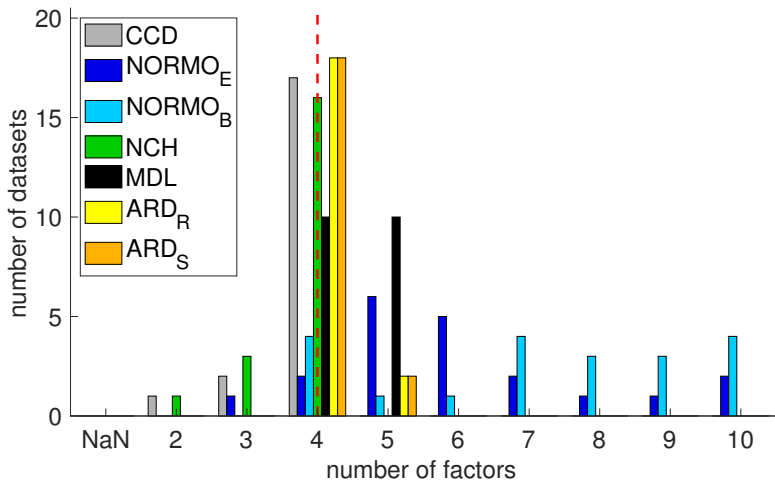
CCD

NORMO_E, NORMO_B

NCH

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Mission 2 - NG_{low} data

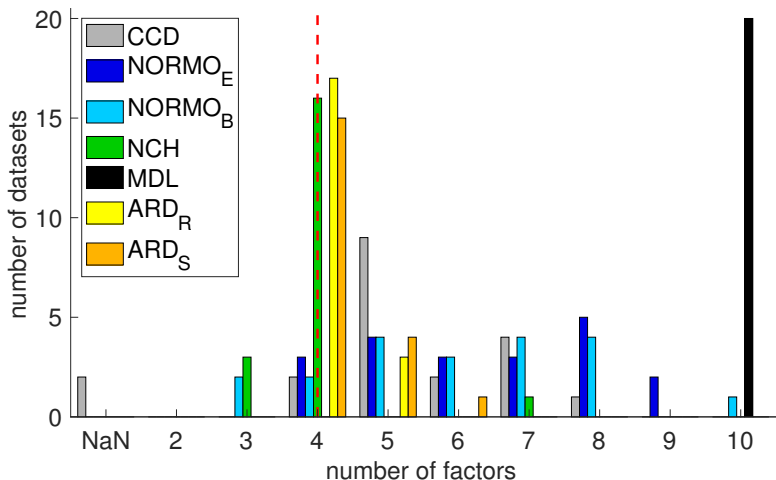
CCD

NORMO_E, NORMO_B

NCH

MDL

ARD_R, ARD_S



Mission 2 - NG_{low} data

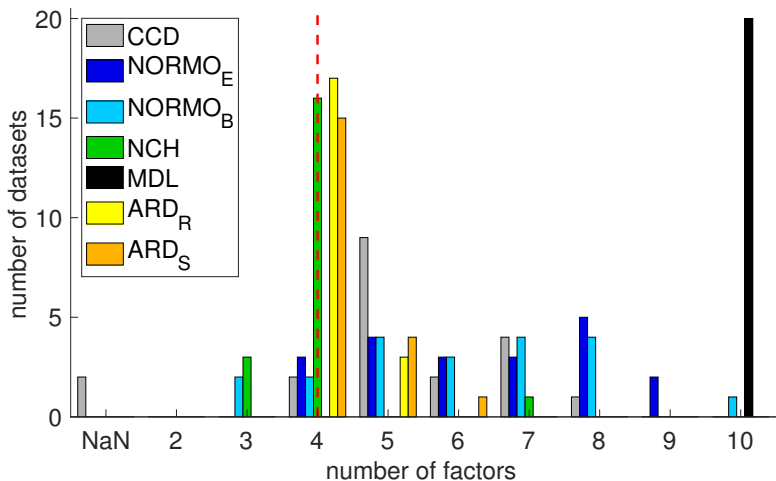
CCD

NORMO_E, NORMO_B

NCH

MDL

ARD_R, ARD_S



Mission 2 - NG_{low} data

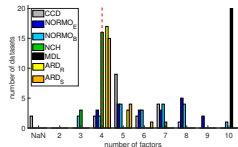
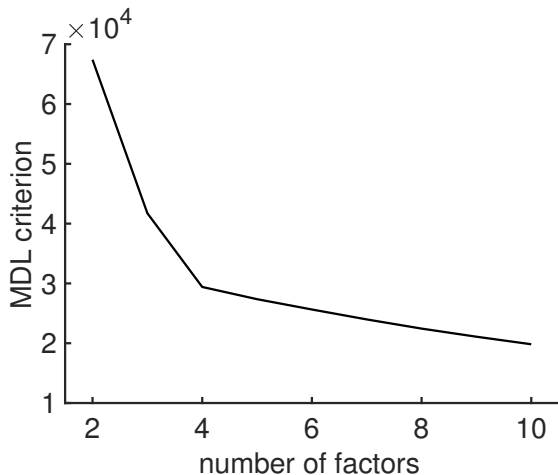
CCD

NORMO_E, NORMO_B

NCH

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Mission 2 - NG_{low} data

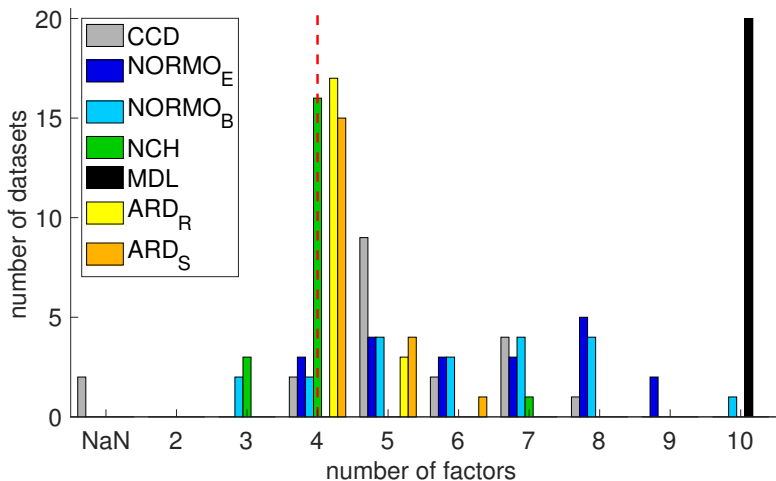
CCD

NORMO_E, NORMO_B

NCH

MDL

ARD_R, ARD_S



Mission 3 - NG_{high} data

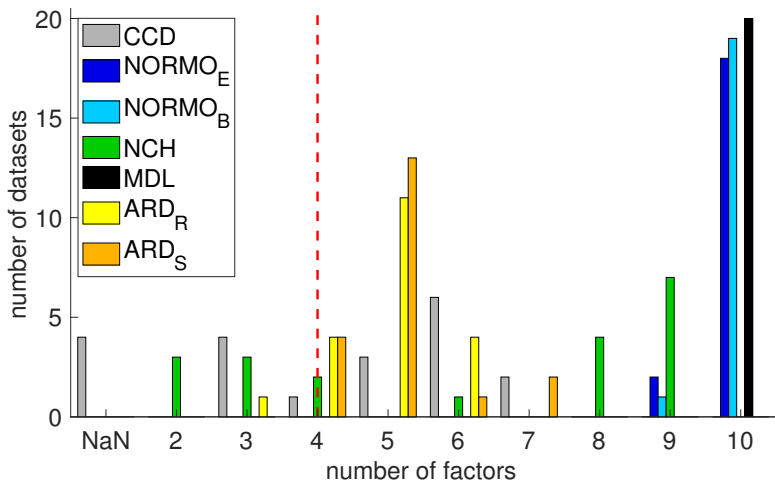
CCD

NORMO_E, NORMO_B

NCH

MDL

ARD_R, ARD_S



Mission 3 - NG_{high} data

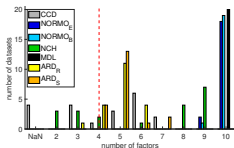
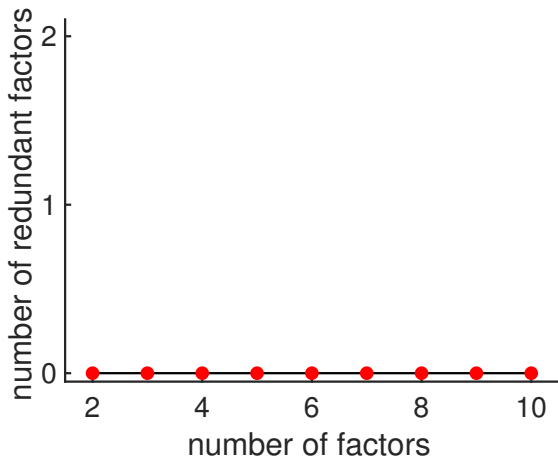
CCD

NORMO_E, NORMO_B

NCH

MDL

ARD_R, ARD_S



Mission 3 - NG_{high} data

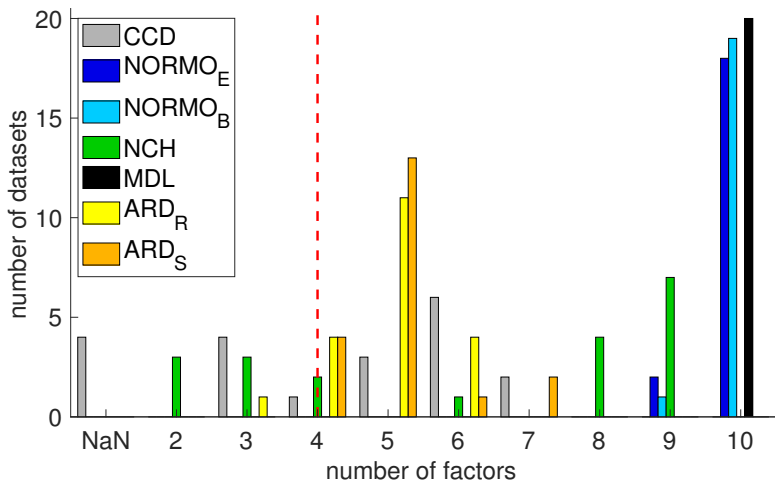
CCD

$NORMO_E$, $NORMO_B$

NCH

MDL

ARD_R , ARD_S



Mission 3 - NG_{high} data

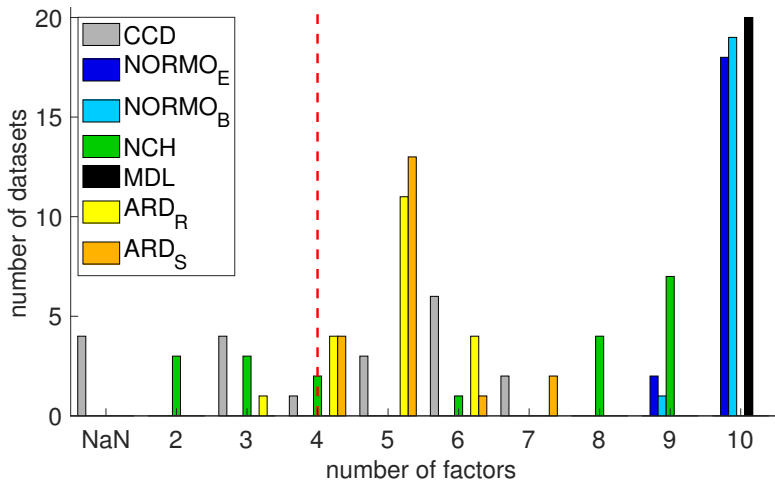
CCD

NORMO_E, NORMO_B

NCH

MDL

ARD_R, ARD_S



Mission 4 - $NBBA_{low}$ data

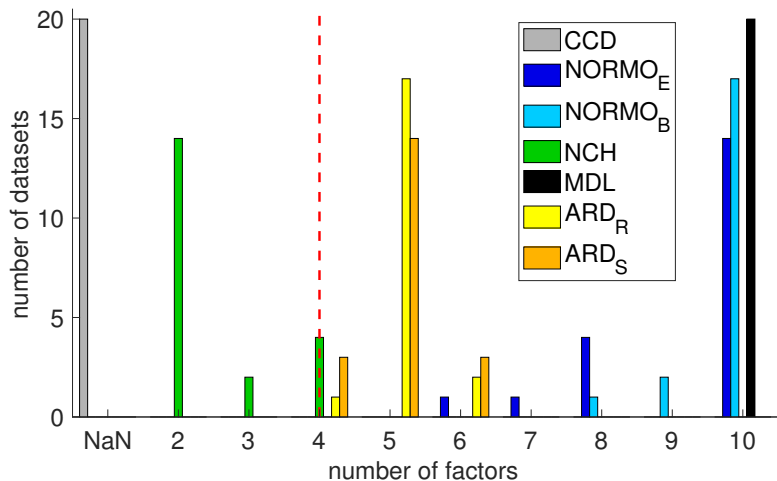
CCD

$NORMO_E$, $NORMO_B$

NCH

MDL

ARD_R , ARD_S



Mission 4 - $NBBA_{low}$ data

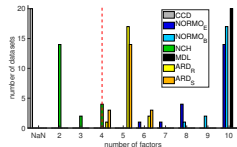
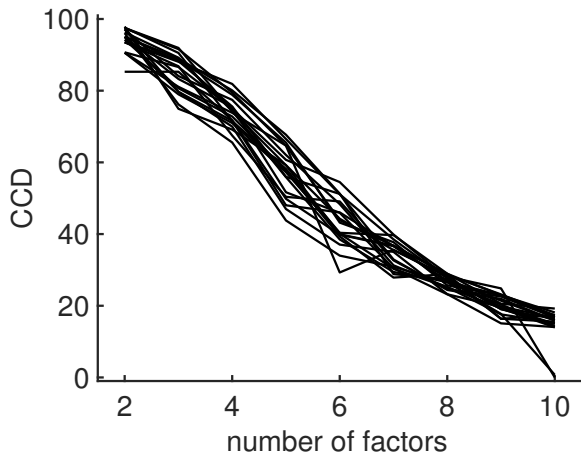
CCD

$NORMO_E$, $NORMO_B$

NCH

MDL

ARD_R , ARD_S



Mission 4 - $NBBA_{low}$ data

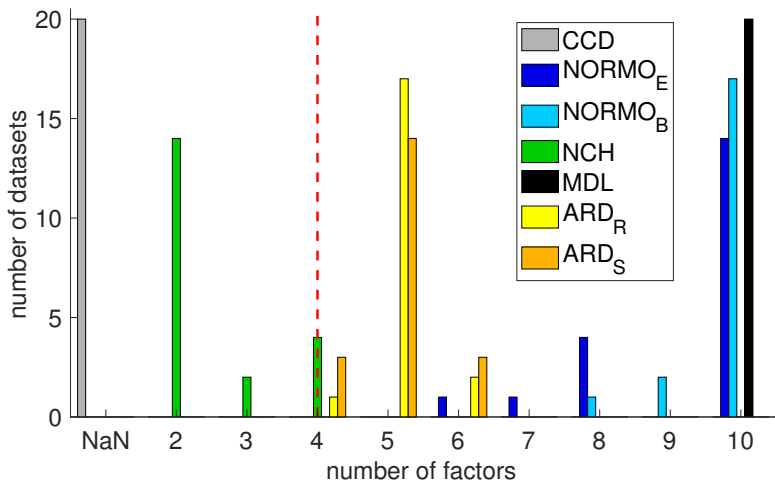
CCD

NORMO_E, NORMO_B

NCH

MDL

ARD_R, ARD_S



Mission 4 - $NBBA_{low}$ data

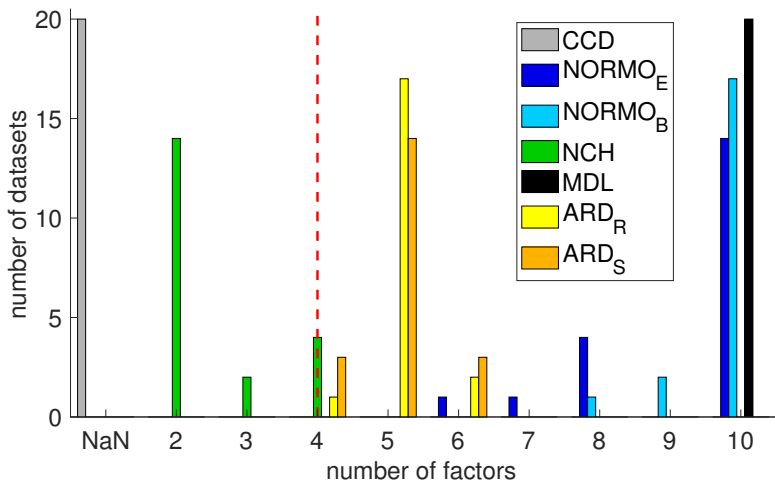
CCD

$NORMO_E$, $NORMO_B$

NCH

MDL

ARD_R , ARD_S



Mission 5 - $NBBA_{high}$ data

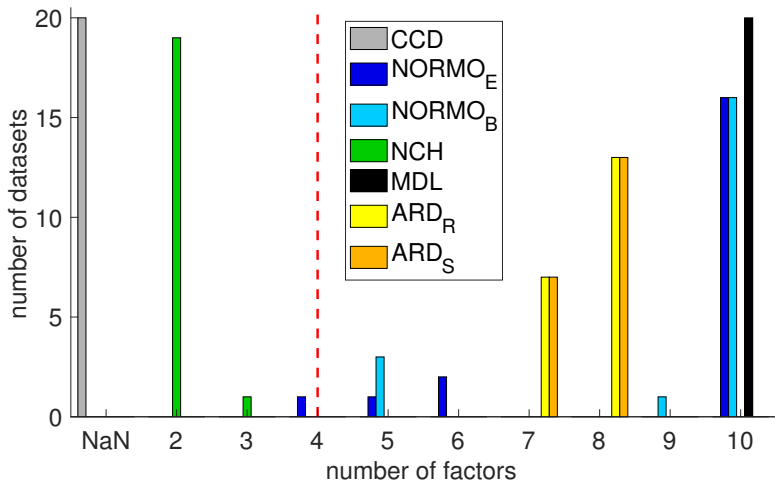
CCD

$NORMO_E$, $NORMO_B$

NCH

MDL

ARD_R , ARD_S



Conclusion: Mission impossible ?

- ⇒ none method produced satisfactory results for PARAFAC decomposition of simulated EEG data
 - **NORMO, MDL** - problems already for noiseless data
 - **CCD** - no visible change-point in CCD due to the gaussian noise/BBA
 - **NCH** - data with BBA $\rightarrow F \approx$ minimal allowed value 2
 - **ARD** - the most promising method \rightarrow modification in the future
- new approaches are needed

Literature



Bro, R. and Kiers, H. A. L. (2003).

A new efficient method for determining the number of components in PARAFAC models.

Journal of Chemometrics, 17(5):274–286.



Ceulemans, E. and Kiers, H. A. L. (2006).

Selecting among three-mode principal component models of different types and complexities: A numerical convex hull based method.

British Journal of Mathematical and Statistical Psychology, 59(1):133–150.



Fernandes, S., Fanaee-T, H., and Gama, J. (2020).

NORMO: A new method for estimating the number of components in CP tensor decomposition.

Engineering Applications of Artificial Intelligence, 96.



Harshman, R. A. (1970).

Foundations of the PARAFAC procedure: Models and conditions for an “explanatory” multimodal factor analysis.

UCLA Working Papers in Phonetics, 16:1–84.



Liu, K., da Costa, J., So, H. C., Huang, L., and Ye, J. (2016).

Detection of number of components in CANDECOMP/PARAFAC models via minimum description length.

Digital Signal Processing, 51:110 – 123.



Mørup, M. and Hansen, L. K. (2009).

Automatic relevance determination for multi-way models.

Journal of Chemometrics, 23(7-8):352–363.



Rošćáková, Z., Rosipal, R., Seifpour, S., and Trejo, L. J. (2020).

A comparison of non-negative Tucker decomposition and Parallel Factor Analysis for identification and measurement of human EEG rhythms.

Measurement Science Review, 20(3):126 – 138.